# A robust separable image denoising based on relative intersection of confidence intervals rule

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Abstract—Many microscopy images, or 3D depth maps can be represented using piecewise constant models. They usually contain noise due to sensor imperfectness. In this paper, an improved separable denoising method based on the relative intersection of confidence intervals rule is proposed. The method uses median averaging and is robust to outliers and different noise distributions. It over-performs competitive methods in the sense of edge preservation.

Keywords—Intersection of confidence intervals; Image denoising; Median; Adaptive filters

#### I. INTRODUCTION

Real-world images usually contain noise (especially in dark areas) due to imperfectness or worth of sensors. Sometimes it is very important to reduce noise, e.g. for astronomy [1], microscopy [2], seismology [3], in medicine, where post-processing methods are more acceptable than higher radiation doses [4].

Wiener filtering is a traditional approach to denoising [5]. Wavelet transform shows good performance, especially for non-stationary images with a piecewise polynomial structure of signals and a non-predictable structure of noise [6][7][8]. If the image has piece-wise constant parts, better approaches are the shape adaptive DCT [9], block-matching and 3D filtering algorithm [10] or intersection of confidence intervals (ICI) rule accompanied with local polynomial approximation [11].

In this paper, we use a robust median based technique for enhancement of the known ICI denoising method.

# II. INTERSECTION OF CONFIDENCE INTERVALS

Let input signal x(n) be corrupted by additive zero mean Gaussian noise w(n). Noise samples are assumed to be independent and identically distributed random variables  $\mathcal{N}(0, \sigma_w^2)$ :

$$y(n) = x(n) + w(n). \tag{1}$$

Our goal is to find a good estimate  $\bar{x}(n)$  of the input signal that accurately restores smooth regions and preserves edges in the same time. Assumption is that the input signal is piecewise constant, so we use zero order estimation on adaptive window length. To obtain the length, we use intersection of confidence

intervals (ICI) rule, which chooses filters with short support near edges and long support otherwise.

In one dimensional application of the ICI rule, we increase window length  $h_k$  until we reach the optimal size  $h^*$  at each observed sample n. Confidence interval is defined for each sample n and for every window length  $h_k$ :

$$D_k(n) = \left[\bar{x}_{h_k}(n) - \Gamma \cdot \sigma_{h_k}(n), \bar{x}_{h_k}(n) + \Gamma \cdot \sigma_{h_k}(n)\right], \quad (2)$$

where  $\Gamma$  is a threshold parameter that defines the confidence interval width and  $\sigma_{h_k}(n) = \sigma_w / \sqrt{h_k}$  is the deviation of the signal sample estimate [12]. The smallest upper and the largest lower confidence interval limits on observed interval are:

$$\begin{split} \overline{L}_k(n) &= \max_{i=1,\dots,k} \Big( \bar{x}_{h_i}(n) - \Gamma \cdot \sigma_{h_i}(n) \Big), \\ \underline{U}_k(n) &= \min_{i=1,\dots,k} \Big( \bar{x}_{h_i}(n) - \Gamma \cdot \sigma_{h_i}(n) \Big). \end{split} \tag{3}$$

Chosen window length  $h^+$  is the largest window length for which the ICI condition

$$\overline{L}_k(n) \le U_k(n) \tag{4}$$

is satisfied. The same rule must be repeated for every sample of y(n).

Typically, we get a slightly too large window lengths using the ICI rule. A good improvement is a relative intersection of confidence intervals rule (RICI) [13][14]. The method is based on ratio of cumulative confidence interval lengths and the size of the current confidence interval:

$$R_k = \frac{U_k(n) - \overline{L}_k(n)}{2\Gamma \sigma_{h_k}}. (5)$$

The chosen window length is the smallest  $h^+ = h_k$  for which is satisfied:

$$R_k < r_c, \tag{6}$$

where  $r_c$  is a preset threshold parameter. The RICI criterion is usually applied as an additional criterion to the ICI rule.

Using all included samples, with respect to window length  $h^+$ , average value on the interval is calculated as:

$$\bar{x}_{h^{+}}(n) = \text{mean} \{y(n), ..., y(n+h^{+}(n)-2), y(n+h^{+}(n)-1)\}.$$
 (7)

In asymptotical sense  $(h^+ \to \infty)$  and if the noise distribution is arbitrary, but symmetrical, mean can be replaced by median:

$$\bar{x}_{h^{+}}(n) = \text{median} \{y(n), ..., y(n+h^{+}(n)-2), y(n+h^{+}(n)-1)\}.$$
 (8)

Such a replacement is less sensitive to choice of  $\Gamma$  and  $r_c$ , and gives more accurate results for almost any noise distribution. Furthermore, outliers in the signal will almost have no influence on the estimation, thus the estimation is more robust. The edges of the signal will be perfectly restored [15]. We introduce the abbreviations MICI (median intersection on confidence interval) and MRICI (median relative ICI).

# III. IMAGE DENOISING ALGORITHM

Zero mean Gaussian noise w(n, m),  $\mathcal{N}(0, \sigma_w^2)$ , is added to the input image x(n, m):

$$y(n,m) = x(n,m) + w(n,m).$$
 (9)

A good method for image denoising is described in [16]. We propose using the same algorithm, but with replacing mean averaging with median averaging to get more robust results. The algorithm consists of three stages:

1. For each pixel y(n,m) observe its row. Find the widest window length on the left side  $h_{rcL}^+(n,m)$  and on the right side  $h_{rcR}^+(n,m)$  from the observed pixel using the ICI or the RICI rule. First letter in an index, r, denotes that the rows are observed first, the second letter, c, means that the columns are observed next, and the third letter symbolizes: L left from the pixel and R right from the pixel. Join all pixels on the intervals and use median:

$$\bar{x}_r(n,m) = \text{median} \left\{ y(n,m-h^+_{rcL}(n,m)+1), \\ y(n,m-h^+_{rcL}(n,m)+2), ..., \\ y(n,m), ..., \\ y(n,m+h^+_{rcR}(n,m)-2), \\ y(n,m+h^+_{rcR}(n,m)-1) \right\}.$$
 (10)

Now, observe each column of the  $\bar{x}_r(n,m)$ . Find the widest window length on upper side  $h^+_{rcU}(n,m)$  and down side  $h^+_{rcD}(n,m)$  from the observed pixel. The third letter symbolizes: U up from the pixel and D down from the pixel. Join the intervals and use median:

$$\begin{split} \bar{x}_{rc}(n,m) &= \text{median} \, \{ \bar{x}_r(n-h^+_{rcU}(n,m)+1,m), \\ \bar{x}_r(n-h^+_{rcU}(n,m)+2,m), ..., \\ \bar{x}_r(n,m), ..., \\ \bar{x}_r(n+h^+_{rcD}(n,m)-2,m), \\ \bar{x}_r(n+h^+_{rcD}(n,m)-1,m) \}. \end{split}$$

2. Now, do the reverse procedure. At the beginning, observe the column for each pixel y(n,m) and find the widest window length up side  $h^+_{crU}(n,m)$  and down side  $h^+_{crD}(n,m)$ . First letter in index, c, denotes that the columns are observed first, the second letter, r, means that the rows are observed next. Calculate estimation  $\bar{x}_c(n,m)$  from pixels in the observed interval:

$$\bar{x}_{c}(n,m) = \text{median} \{ y(n - h_{crU}^{+}(n,m) + 1, m), \\ y(n - h_{crU}^{+}(n,m) + 2, m), ..., \\ y(n,m), ..., \\ y(n + h_{crD}^{+}(n,m) - 2, m), \\ y(n + h_{crD}^{+}(n,m) - 1, m) \}.$$
 (12)

Then, observe each row of the  $\bar{x}_c(n,m)$ . Find the widest window length on the left side  $h^+_{crL}(n,m)$  and on the right side  $h^+_{crR}(n,m)$ . Calculate estimation  $\bar{x}_{cr}(n,m)$  using median:

$$\begin{split} \bar{x}_{cr}(n,m) &= \text{median} \, \{ \bar{x}_c(n,m-h_{crL}^+(n,m)+1), \\ \bar{x}_c(n,m-h_{crL}^+(n,m)+2), ..., \\ \bar{x}_c(n,m), ..., \\ \bar{x}_c(n,m+h_{crR}^+(n,m)-2), \\ \bar{x}_c(n,m+h_{crR}^+(n,m)-1) \}. \end{split} \tag{13}$$

3. Combine estimated images  $\bar{x}_{rc}(n,m)$  and  $\bar{x}_{cr}(n,m)$  to the final denoised result. The simplest way is averaging the two estimates:

$$\bar{x}(n,m) = (\bar{x}_{rc}(n,m) + \bar{x}_{cr}(n,m))/2.$$
 (14)

We denote it as MRICI method with fixed weights. More accurate way is to take weighting factors that depend on reliability of each estimate (MRICI method with the variable weights) [12][16]:

$$\omega_{rc}(n,m) = h_{rcL}^{+}(n,m) + h_{rcR}^{+}(n,m) + h_{rcD}^{+}(n,m) + h_{rcD}^{+}(n,m),$$

$$\omega_{cr}(n,m) = h_{crL}^{+}(n,m) + h_{crR}^{+}(n,m) + h_{crD}^{+}(n,m),$$

$$\bar{x}(n,m) = \frac{\omega_{rc}(n,m) \cdot \bar{x}_{rc}(n,m) + \omega_{cr}(n,m) \cdot \bar{x}_{cr}(n,m)}{\omega_{rc}(n,m) + \omega_{cr}(n,m)}.$$
(15)

Proposed method characterizes edge preservation, which is an important feature in the image denoising. Final image is less sensitive to statistical deviations (e.g. outliers) in the image and to sudden changes in the neighboring pixel values. Resulting image has less oscillation near edges. Therefore, it is sharper than when achieved using comparable methods.

Simulation results of the proposed method are presented in the following chapter.

### IV. SIMULATION RESULTS

The example is 64x64 pixels test image. It contains gray scale blocks (Fig. 1(a)) and additive zero mean Gaussian noise  $\sigma_w = 10$  (Fig. 1(b)). We performed separable image denoising method based on the intersection of confidence intervals rule using mean and a threshold parameter  $\Gamma = 4.4$ . Final estimated image is calculated using fixed and variable weights (Fig. 1(e) and (f), respectively). Artifacts of separable approach are clearly visible; rows and columns are outstretched. If we replace mean by median inside the ICI rule, we get Fig. 1(g) and (h). The rows and columns are less outstretched, but the edges between different gray shades are not perfectly restored. Fig. 1(i) and (j) shows the estimate calculated using fixed and variable weights and mean based RICI method  $\Gamma = 4.4$  and  $r_c = 0.85$ . The best results are achieved when mean is replaced by median (Fig. 1(k) and (l)). Edges are almost completely preserved and true pixel values are accurately restored.

We compare our results with the anisotropic LPA-ICI,  $\Gamma=1.05$  [17] and non-decimated Haar wavelets (hard threshold  $3.5\sigma_w$ , 4 decomposition levels) as shown in Fig. 1(c) and (d). In both cases, visual results are worse than in any of the proposed methods. Background is not smooth, and the edges are not sharp.

In Fig. 2(a),(f) the same test image is presented, but with different noise distributions: Laplacian and binomial. Both noisy images are denoised using the anisotropic LPA-ICI method ((b), (g)), undecimated Haar wavelet transform ((c),(h)), mean and median RICI with the fixed weights ((d)-

(e), (i)-(j)). In the binomial noise case, the MRICI gives an almost perfectly reconstructed image, while the RICI solution is biased – it gives wrong gray shade level.

Fig. 3 shows PSNR-s for mentioned methods (LPA-ICI, undecimated Haar wavelet transform, separable mean RICI and proposed separable median RICI (MRICI) with fixed weights) for additive Gaussian, Laplacian and binomial noise for noise deviation range of  $\sigma_w \in [0,100]$ . Separable RICI method results in better PSNR-s for smaller  $\sigma_w$ . Undecimated Haar wavelet and anisotropic LPA-ICI methods show the best results for high levels of the noise. The MRICI outperforms the mean RICI for the lower level of the noise, especially for the additive binomial noise.

In TABLE I. peak signal to noise ratios are compared for the same test image and for three noise distributions: Gaussian, Laplacian and binomial, 30 realizations of each. All noise distributions are zero mean and have  $\sigma_w = 10$ . In all cases, the new proposed methods show the best PSNR results.

#### V. CONCLUSION

In this paper we have proposed two novel methods for image denoising which are based on the relative intersection of confidence interval rule and a robust median estimator. They give larger PSNR-s than competitive methods for different noise distributions. They offer better edge preservation and are less sensitive to outliers in the noisy image.

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TABLE I. PSNR FOR 30 REALIZATIONS OF THE TEST IMAGE AND THREE DIFFERENT NOISE DISTRIBUTIONS: GAUSSIAN, LAPLACIAN AND BINOMIAL.

|                        | Gaussian<br>noise, dB | Laplacian<br>noise, dB | Binomial<br>noise, dB |
|------------------------|-----------------------|------------------------|-----------------------|
| noisy-image            | 28.1372               | 28.1263                | 27.7333               |
| ICI, fixed weight      | 19.5834               | 19.5659                | 19.7396               |
| ICI, variable weight   | 19.5706               | 19.5530                | 19.7269               |
| MICI, fixed weight     | 28.1511               | 28.1373                | 27.7886               |
| MICI, variable weight  | 28.1523               | 28.1405                | 27.7762               |
| RICI, fixed weight     | 40.8962               | 38.9303                | 36.3624               |
| RICI, variable weight  | 40.7430               | 39.0041                | 36.2947               |
| MRICI, fixed weight    | 42,1992               | 40.1020                | 42.6739               |
| MRICI, variable weight | 41.8532               | 40.1671                | 42.3026               |
| anisotropic LPA-ICI    | 39.9478               | 37.3952                | 35.5632               |
| Haar wavelet           | 40.4542               | 39.7961                | 35.9131               |

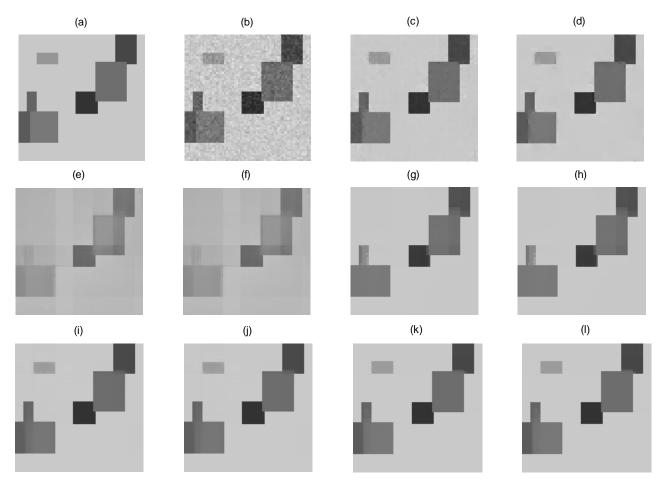


Fig. 1. (a) Test noise free image. (b) Noisy image with zero mean Gaussian noise  $\sigma_w = 10$ . (c) Anisotropic LPA-ICI denoised image with  $\Gamma = 1.05$ . (d) Undecimated Haar wavelet denoised image with hard threshold  $3.5\sigma_w$  and 4 decomposition levels. (e) Mean ICI ( $\Gamma = 4.4$ ) with fixed weights denoised image. (f) Mean ICI ( $\Gamma = 4.4$ ) with variable weights denoised image. (g) Median ICI ( $\Gamma = 4.4$ ) with fixed weights denoised image. (h) Median ICI ( $\Gamma = 4.4$ ) with variable weights denoised image. (i) Mean RICI ( $\Gamma = 4.4$ ,  $r_c = 0.85$ ) with fixed weights denoised image. (l) Median RICI ( $\Gamma = 4.4$ ,  $r_c = 0.85$ ) with fixed weights denoised image. (l) Median RICI ( $\Gamma = 4.4$ ,  $r_c = 0.85$ ) with variable weights denoised image.

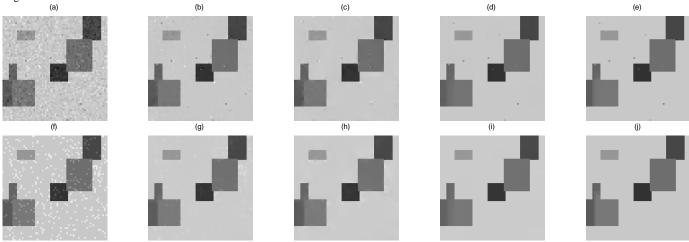


Fig. 2. (a) Image with added Laplacian noise  $\sigma_w = 10$ . (b) Anisotropic LPA-ICI denoised image with  $\Gamma = 1.05$ . (c) Undecimated Haar wavelet denoised image with hard threshold  $3.5\sigma_w$  and 4 decomposition levels. (d) Mean RICI ( $\Gamma = 4.4, r_c = 0.85$ ) with fixed weights denoised image. (e) Median RICI ( $\Gamma = 4.4, r_c = 0.85$ ) with fixed weights denoised image with  $\Gamma = 1.05$ . (h) Undecimated Haar wavelet denoised image with hard threshold  $3.5\sigma_w$  and 4 decomposition levels. (i) Mean RICI ( $\Gamma = 4.4, r_c = 0.85$ ) with fixed weights denoised image. (j) Median RICI ( $\Gamma = 4.4, r_c = 0.85$ ) with fixed weights denoised image.

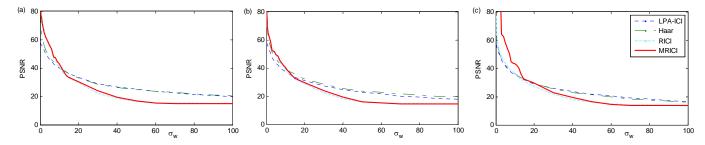


Fig. 3. PSNR as a function of  $\sigma_w$  for different denoising methods and different noise distributions: (a) Gaussian noise, (b) Laplacian noise and (c) binomial noise.

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